

The functional matrix hypothesis revisited. Orofacial capsular matrices defined

Timothy G. Bromage, BA, MA, PhD

Department of Molecular Pathobiology, New York University College of Dentistry, New York;
Professor

Timothy G. Bromage

Department of Molecular Pathobiology

New York University College of Dentistry

345 East 24th Street

New York, NY 10010

USA

Tel: +1 212 998 9597 (office)

+1 212 289 4534 (home)

Fax: +1 212 995 4445

Email: tim.bromage@nyu.edu

The functional matrix hypothesis revisited. Orofacial capsular matrices defined

Highlights

Descriptions of the orofacial capsular matrices are incomplete.

The functional matrix of the oral cavity is hard and tough food.

The functional matrix of the nasal cavity is air.

ABSTRACT

The functional matrix hypothesis was introduced by Melvin L. Moss in the 1960's, and has been an enduring concept for explaining the compensatory growth and development of the craniofacial complex in general, and the facial skeleton in particular. It remains true in concept, but we maintain it is incomplete. Functional matrices are of two types: periosteal matrices comprise muscle/tendon attachments to skeletal units, and capsular matrices enclose a tissue mass or volume within a functional space. Regarding the latter, pressure arising from growing contents of the neurocranial capsular matrix explain the expansion of the braincase. However, expansion of orofacial capsular matrices are said to be intrinsically-derived spaces that satisfy the metabolic demands of the body. We offer support for the idea that these capsular matrices have contents that furnish the pressures required to form these spaces. The oropharyngeal capsule is mechanically challenged by chewing a hard and tough diet, and in so being challenged grows sufficiently to render a normal occlusion. The functional matrix of the oral cavity is hard and tough food. The nasopharyngeal capsule is mechanically challenged by air pressures elicited by vigorous nasal breathing. While chewing forces likely also play a role in development of the

nasopharyngeal passage, nasal breathing is suggested to be primary. The functional matrix of the nasal cavity is air. The orthodontic community must transition from treating only the symptoms of perturbed facial growth, to acknowledging the public health benefit of identifying the causes of maxillary and mandibular insufficiencies and tooth crowding.

INTRODUCTION

Conceptualization of the functional matrix hypothesis (FMH) by Melvin L. Moss remains a pillar of orthodontic theory as an explanation for compensatory growth of the craniofacial skeletal complex principally in response to the growth and function of soft tissue matrices. Excellent historical accounts of this concept may be found in the literature ¹⁻⁴. The expression “functional matrix” was introduced to the orthodontic community and described by Moss in 1962 ² as a tissue mass enclosed by bones to form a functional unit. This concept was operationalized in an analysis of the developing maxilla in 1967 ⁵. In the following year, whilst performing a functional analysis of the mandible, the FMH concept adopted a more complete view, detailing the primacy of the functional matrix to elicit secondary growth responses by its corresponding skeletal unit ⁶. In that study, *teeth* were introduced as the functional matrix of the alveolar skeletal unit of the mandible. It is also noteworthy that while Moss described the FMH at the macro scale, in this publication he referred to supporting research on bone growth remodeling at the microscopic scale by Enlow ⁷. The support and strength that this dyad provided would become a staple of developing theory in publications by both Moss and Enlow throughout their careers.

In 1969 Moss and Moss-Salentijn formalized the capsular matrix ⁸ and provided the relatively advanced explanation of the FMH that remains the core of the concept today ⁹. Functional matrices were said to be of two types; periosteal matrices serve as the functional muscle/tendon attachments to skeletal units, and capsular matrices enclose a mass or volume within a functional space. Because it is easy to intuit, the neurocranial capsular matrix was heralded to convey the concept of the FMH. However, an operational description of the oronasopharyngeal functional space was needed ⁸:

Operationally, the form (the size and the shape) as well as the spatial location of the orofacial capsule, and therefore of any of its completely embedded and included functional cranial components, is determined primarily by the operational volumetric demands of the enclosed patent functioning spaces. (p. 478).

For the moment, we wish to state only that the human oronasopharyngeal functioning space alters in size alone, not in shape, after the beginning of the third month of pregnancy. This morphogenetically primary volumetric increase causes a compensatory increase in the size of the orofacial capsule. Growth of the enveloping capsule is produced by mitosis of both its epithelial and mesenchymal cellular elements and the consequent increase in intercellular materials, which results in an

expansion of the capsule as a whole. Within the capsule are situated a number of mandibular functional cranial components, periosteal matrices together with their respective skeletal units. (p. 483).

The operational demands of the respiratory and digestive systems creating patency of the oronasopharyngeal functional space were aptly described as related to the metabolic demands of the body ⁸. Attributes of the capsular matrices themselves were not described, other than to claim primacy as an intrinsic space, a throughway, from which its tissue boundaries grew mitotically from early embryonic life. Therein is the first irony that partly prompted this communication. It is well understood that anomalies of functional matrices are responsible for abnormal growth, such as was discussed by Moss regarding defects in neural mass ¹⁰. Then why do perfectly normal teeth that comprise the functional matrix of the alveolar bone become crowded? If growth of the oronasopharyngeal functional space is intrinsic, then why are there anomalous mismatches between large tongues and relatively small oral volumes? Despite these and other questions, we are sure Moss would have agreed that extrinsic environmental factors were at work. If so, it suggests that the orofacial capsular matrices that make up the oronasopharyngeal functional space do in fact contain something, and until we describe what that something is, the FMH remains incomplete.

The position taken in this communication is that growth of the orofacial capsular matrices must be explained in exactly the same fashion that Moss and colleagues have described for the neurocranial capsular matrix, which is an enclosure having contents that exert pressure, which in turn stimulates compensatory growth of its skeletal unit.

Above we mention one reason for undertaking the present analysis. The other reason concerns the opening three sentences of Moss and Moss-Salentijn's 1969 paper on the capsular matrix ⁹, which was a shout-out from the basic sciences to the orthodontic community, that a knowledge and theory of cranial growth is fundamental to clinical practice:

It is commonly agreed that a comprehensive knowledge of cranial growth is a sine qua non for any rational approach to orthodontic therapy. Quite apart from the intrinsic value of such information, many aspects of orthodontic diagnosis, therapy, and prognosis are based firmly on this aspect of cranial biology. Far from being an academic matter, it is easily demonstrated that the fundamental conceptualizations of the orthodontist concerning the process of cranial growth strongly influence his therapeutic techniques. (p. 474).

If it was commonly agreed in 1969, it is no longer. The orthodontic community failed to appreciate this guidance. Interactions with postgraduate residents in orthodontics from around the world largely inform us that 1) if at all, they vaguely recall the names Moss and Enlow from school (most have not read the literature); 2) irrespective of this, they do not understand fundamental principles of bone growth, let alone craniofacial bone growth; 3) they do not know

what teeth are for; and 4) they do not understand the role of respiration in facial growth. Therein emerges the second irony prompting this communication, which is that such knowledge and theory would have helped to mitigate the mishaps of orthodontic therapy, such as relapse, root resorption, failure to achieve desired tooth movement(s), and more, as recently reviewed in this journal ¹¹. More significantly, such knowledge and theory would have been used in campaigns to reduce the prevalence of dental crowding, maxillary and mandibular insufficiencies, and other craniofacial skeletal anomalies in the general public; orthodontics would have transitioned to preventative dental medicine, thus minimizing iatrogenic harm.

Following are descriptions of the contents of orofacial capsular matrices in order that the FMH may be better understood and hopefully applied in clinical orthodontics.

The oropharyngeal cavity

To understand what contents fill and regulate growth of the oropharyngeal cavity, we must address the 3rd deficiency of understanding mentioned above.

What are teeth for? Human enamel is a biological material made of approximately 95% by weight carbonated hydroxylapatite $\text{Ca}_{10}(\text{PO}_4)_6(\text{OH})_2$ (hydroxyapatite), with the remaining 3-4% being protein and a 1-2% fraction of water. The hierarchy of attributes that convey mechanical efficacy from the macro- to the nanoscopic scale of enamel will reveal attributes of the functional matrix. At the macroscopic end of the spectrum are the loads and stresses absorbed by an intact tooth due to the incursive, intercuspal, and excursive contacts that distinguish an individual's unique masticatory function ¹².

A level down the hierarchy is enamel thickness. Human enamel is among the thickest of all primates, being 2 mm thick and more on molars ¹³. This is an adaptation to a hard and tough diet ¹⁴ in order to survive the lifetime of wear. Until the exposure of dentine, enamel also retains highly decussated enamel prisms, or rods, at the inner enamel. Mammalian species with hard and tough diets develop this architecture wherein groups of enamel prisms cross at some angle to one another and are observed as Hunter-Schreger bands (HSBs) ^{15,16}. Human molar HSBs originate at the enamel-dentine junction (EDJ), coursing toward the outer enamel but typically dispersing into a zone of parallel rods before reaching the surface in an unworn tooth ¹⁶. In the lower enamel, the junctions between decussating groups of prisms forms an enamel prism discontinuity that serves to resist the propagation of cracks ¹⁷. Occlusal loads drive the enamel shell into the significantly softer underlying dentine, causing peak tensile stress of the enamel situated at the EDJ, to which brittle solids like enamel are vulnerable. The HSBs and their enamel prism discontinuities are thus situated in exactly that region of the enamel volume to serve as an adaptation to resist the propagation of bottom surface cracks ^{18,19}.

Prism orientation at wear surfaces also confers resistance to load and functional wear²⁰⁻²³ especially as regards a diet of hard and tough food. Adaptations of prism orientation have been shown to vary in relation to dietary niches of early humans²⁴.

When materials embody a sharp transition in density, differential strains cause fracture or separation at the transition under load. Human molar enamel thus contains another discontinuity in a zone whose gradients in hardness and elastic modulus diminish from the outer surface toward the inner enamel²⁵, the enamel becoming more compliant at the EDJ. The dentine side of the EDJ is itself graded too, it initially having mechanical properties quite similar to enamel, but then becoming softer and more stress-tolerant some tens of micrometers away from the EDJ²⁶⁻²⁸. This is an adaptation to a diet of hard and tough food.

There are further enamel discontinuities at the microscopic scale that confer mechanical efficacy^{21,29}. Enamel prism structures are about 5 μm in diameter, which are packed with crystallites around 20-40 nm in width. The crystallographic *c*-axes of these crystallites are formed perpendicular to the secretory surface of the ameloblast's Tome's process. Because this process is asymmetrical, a complex arrangement of crystallite orientations within prisms creates enamel crystallite discontinuities at the junctions between prisms²⁹. These discontinuities are anti-crack propagating at the micrometer scale. Enamel crystallites are hexagonal and are packed so that their flat surfaces against one another will provide sliding planes at the nanometer scale, offering resistance to strains in bulk enamel by absorbing stress under high biological loading conditions. Cracks that might emerge at the nanometer scale will also arrest at this length scale among the discontinuities between crystallites.

Finally, ameloblast secretory behavior renders incremental lines over daily and near-weekly timescales in humans that produce changes in mineralization chemistry^{29,30}, producing compositional discontinuities. In addition, low mineralization density due to porosity, putatively at prism boundaries and their centers³¹, is yet another density-dependent discontinuity, which confers mechanical resistance to loading.

In sum, the macro- to nanoscopic arrangement of discontinuities in structure and composition renders human enamel supremely competent at absorbing stresses in the biological loading stress regime encountered with a hard and tough diet. Fractures that may begin at the nanoscopic scale will follow paths of least resistance indicated by the various discontinuities described³². The heterogeneity of these discontinuities enables enamel to arrest cracks before becoming catastrophic.

Human teeth are designed for processing hard and tough foods.

What is the relationship between what teeth are for and their bone? It is an axiom of hard tissue biology attributed to Wolf's Law³³ that bone adapts its architecture to the habitual intensity and frequency of mechanical loads to which it is subject. Frost³⁴ specifically targeted

an explanation of Wolff's Law to the orthodontic community to enhance the clinicians' understanding of its concepts. Mechanically-mediated effects by biological loads and mildly overloaded biological regimes will have a positive effect on bone growth. We are speaking of sufficient mechanical forces transmitted through teeth, that is, through the enamel, EDJ, dentine, periodontal ligament, and ultimately to the maxillary and mandibular bones, which experience the stress and strains that stimulate growth and expand the oral cavity and oropharynx. In both the child and the non-grower, orthodontic tooth movement is only possible because of the maxillary and mandibular bone threshold for receiving mildly overloaded forces to enable modeling drift of the tooth through tissue space. These concepts dominate much of the basic science and clinical literature on bone, particularly in respect to exercise, e.g. ³⁵⁻³⁷.

Underloading has no effect on modeling drift to change shape or increase bone size ³⁴. A bone that does not experience the strain thresholds to which it was adapted during growth will not stimulate modeling sufficiently to increase in size to its genetic potential. Underloading of the jaws will cause maxillary and mandibular insufficiencies and tooth crowding. Biological loading and mildly overloaded force regimes will subject a bone to strains that promote size and shape change consistent with the demands of the mechanical environment ³⁸. Meeting or mildly exceeding the biological strain threshold of the jaws will cause the maxillary and mandibular bones to grow sufficiently and to permit all teeth to erupt into a normal uncrowded occlusion.

To understand what mechanical environment human teeth and maxillary and mandibular bones are adapted to, modern-day hunters and gatherers provide the grist for a comparison of their diet with industrialized people. In a study of the Hadza people of northern Tanzania, the average fracture toughness of various underground plant species consumed was about 2000 Jm² ³⁹, even after processing by roasting to make the food softer. In a sample of store-bought cheeses, vegetables, and nuts typically available in the industrialized world, the average fracture toughness is roughly 200 Jm² ⁴⁰, the highest value of 647.9 Jm² given for the green turnip. There is an order of magnitude difference between the mechanical properties of what the Hadza eat and what is available to industrialized people. But as both communities of people process their food, this may reveal a common human behavioral response to effect a reduction in mechanical properties, perhaps because of the metabolic cost associated with mastication. We know that orofacial muscle tonus is positively associated with mechanical food properties ⁴¹. A focus group asked to rate the preferred cooking time of noodles chose around 7 minutes in boiling water, which is at just that moment when they reach the minimum toughness value of about 140 Jm² from the uncooked value of about 200 Jm² ⁴². Wikipedia provides many benefits and drawbacks to food processing except what is the most important in this regard, which is the omission that processed foods are invariably less hard and tough ⁴³.

The line of argument above leads us inextricably to conclude that the overwhelming prevalence of maxillary and mandibular insufficiencies and commensurate tooth crowding in the industrialized world is linked to a reduction in the mechanical properties of the diet. As in all

biological systems, there is variability in tooth size, bone size, and the capacity for what Enlow called “intrinsic compensation”⁴⁴ that will permit some people to avoid a problem when it appears they should have one, and for others to have a problem when by all measures they shouldn’t. Reasons for this require research, but the vast majority of craniofacial skeletal anomalies of interest to the orthodontist mentioned above can be explained by deficiencies in the mechanical properties of the diet alone.

The functional matrix of the oral cavity is hard and tough food.

The nasopharyngeal cavity

To understand what contents fill and regulate growth of the nasopharyngeal cavity, we must address the 4th deficiency of understanding mentioned above.

What is the role of respiration in facial growth? We can address this question by outlining its physiologically important attributes in connection with the necessary exchange of carbon dioxide and oxygen to meet the metabolic demands of the body, and olfaction⁴⁵⁻⁴⁹: *humidity* added to the inspired air facilitates lung function; *nitric oxide* release in the upper respiratory tract destroys pathogens and assists in the regulation of carbon dioxide and oxygen concentrations; *filtering* of particulates from the air protects the lung’s delicate structures; *thermal conditioning* of the air by warming facilitates gas exchange in the lungs; *vagal tone* is stimulated during deep diaphragmatic breathing and facilitates health; *immune defenses* are mounted against airborne pathogens.

What distinguishes these features and benefits of the airway as a group is that none of them occur during habitual mouth breathing, but rather describe the purpose of obligate nasal breathing. It is universally appreciated that all mammals are obligate nasal breathers, yet metabolic demands beyond resting levels are said to induce a switch in humans to obligate mouth breathing⁵⁰.

...the onset of oronasal breathing...was quite consistent individually, but varied considerably between individuals without showing a significant sex difference. The factors most closely related to the switching point were rating of perceived exertion of breathing and nasal work of breathing. (p. 61).

It is extremely unfortunate that our scientific community so readily accepted this line of research without question (e.g.,⁵¹), but it is understandable because, just as humans endeavor to make chewing easy (see section above), so they attempt to make breathing easier too.

Two clues from the quote above illustrate the misapplication of the study results to airway research. The first clue is the considerable variability between subjects independent of sex. If a

normal healthy population were sampled, and the switch to obligate mouth breathing was a human metabolic adaptation, then why the tremendous variability between individuals? The second clue is the "perceived" exertion as a function of nasal resistance, which study subjects took to mean more work than necessary, which then caused the switch to mouth breathing despite the important biological functions described above.

That this misapplication continues today defies logic and illustrates where improvements can be made in orthodontic dental education. Implicit in the first clue above is that the variability among subjects exists because their normal biology, behavior, and health has been modified in whatever direction each individual experienced less respiratory work. They will vary because of the length and duration of their maladaptation, intrinsic facial morphological variability, and their differences in flexibility of metabolic rate. Anomalies of facial development and dental health attributed to mouth breathing - typically in relation to nasal obstruction - include aberrant inferoposterior mandibular rotation, overjet, long face, narrowing of the dental arches, overcrowding, open bite, cross bite, poor lip seal and posture, and relatively small external nares,⁵²⁻⁶³ outcomes that have been largely experimentally induced in a primate model^{64,65}, and which are universally regarded as harmful to health.

Implicit in the second clue above is that, while nasal breathing is more work⁶⁶, it is less efficient. This year in a study of recreational runners purposefully trained to breathe through their nose during intense exercise, both mouth and nasal breathing were examined for carbon dioxide and oxygen exchange⁴⁶. It was found that the ratio of oxygen intake to carbon dioxide outtake lowered in nasal breathing, suggesting that oxygen was given more time to enter and remain in the bloodstream while at the same time tolerating higher concentrations of carbon dioxide. This is a measure of performance and endurance that benefits nasal breathers and elite athletes. Thus while mouth breathing divests more carbon dioxide during intense exercise, which at first appears to relieve the oxygen debt, it actually makes the oxygenation of our cells more difficult. It is interesting that once trained, any deficits that may otherwise be attributed to nasal breathing are eliminated. Erect posture and exercise actually decrease nasal resistance^{67,68}, which is another expression of our adaptation.

To appreciate why humans have maintained the biological necessity explicit in the mammalian adaptation for nasal breathing, one only has to account for our origins in the Great African Rift Valley⁶⁹. Landscapes then, several million years ago, and now, contained a variety of habitats, but aridity is a common feature of many of them for various durations of the year. Water loss in the switch from nasal to mouth breathing increases by 42%⁷⁰, which is potentially deadly, particularly during water scarcity. Anyone watching people run across these African landscapes in remote parts of the continent will not have observed any mouth breathing. Elite long distance runners, except perhaps for the final push to the finish line, are also habitual nasal breathers. Amateur runners accompanying the elites in marathons will include many mouth breathers who are losing so much water vapor that the route's water stations cannot be close enough together.

The selection pressure to preserve water is by itself extreme enough to explain human nasal breathing history. It is no wonder that facial growth is perturbed and that dental health is compromised by aberrant "obligatory" mouth breathing, something humans were never adapted to perform.

Obligatory nasal breathing is for promoting normal facial growth and function.

What is the mechanism relating nasal breathing to growth of the facial skeleton?

Regrettably, the research required to solidify an answer to this question does not exist. However, together with our reasoning outlined in the section above, the circumstantial evidence given below strongly suggests that the answer is yes.

Resistance to nasal airflow is borne by the mucosa and other soft tissues overlying bone of the nasal passage. The resistance is not insignificant, requiring about 50% more effort than required for mouth breathing ⁶⁶. (it is no wonder that indolent energy-unconscious individuals switch to mouth breathing when physically challenged by exercise).

The results of airflow studies in the literature vary depending upon anomalies of nasopharyngeal anatomy, but geometry-based simulated breathing flow rates vary from roughly 2 to 8.5 m/s, depending on location, being highest at the nasopharynx ^{45,66,71}. Because of anatomical variations within the nasal passage and the influence that turbinates have on flow patterns, pressure varies from roughly -9 Pa to 7 Pa ^{45,71}, with nasal mucosal wall shear stresses reaching about 1 Pa ^{45,72}. All values are expected to be significantly higher during intense physical exercise, and while this has not been modeled, turbulent nasal airflow is said to occur above 40-80 Pa ^{49,73}.

We thus anticipate pressure differences during cyclic nasal breathing to be in the vicinity of 100 Pa (=10,000 nN) and higher during intense physical exercise. Bernoulli forces of this magnitude represent 10 grams of compression pressure per square centimeter. This is many orders of magnitude larger than the 100-500 nN proliferative pressure exerted by growing tissues on their surroundings ⁷⁴. The airway is incessantly subject to cyclic mechanical stresses such as compression, shear, and stretch during breathing ⁷⁵. Cyclic stretch in particular is recognized as one factor mediating cell proliferation ^{76,77}.

Growth in body mass is linearly related to increases in metabolic rate. Assuming ideal nasal breathing during development, nasal passages must increase in size to maintain homeostasis consistent with higher metabolic rates. Increased ventilatory demand at larger sizes may in tandem increase nasal resistance and increased pressures that stimulate growth. However we rather think that the Bernoulli forces at high levels of physical activity, as might occur during vigorous play, stimulate the increase in size of the nasal soft and hard tissues. We posit that high intranasal pressures may expand the nasal passage, distending sutures that absorb much more of

the strain energy than the surrounding bone ⁷⁸, leading to compensatory modeling of sutures and the delicate bones of the nasal region.

Diet and the nasal cavity. We do not discount the contributions from chewing a hard and tough diet on the size of the nasal cavity for a few additional reasons. 1) The high principle tensile strains noted over sequential cross sections of the human nasal passage ⁷⁹ will distend the sutures during growth that then respond by compensatory modeling. 2) The number of chews is significantly decreased during mouth breathing compared with nasal breathing, which may reduce the mechanical environment and lead to malocclusion ⁸⁰. 3) The anthropological literature notes that a variety of skulls ranging from the eleventh-eighteenth centuries exhibit a correlation between nasal breadth and the distance between the canines of the upper jaw ⁸¹; these people surely had a significantly harder and softer diet than present day industrialized people. We do not discount these mechanical explanations, but because orthodontic maxillary expansion in the grower does not significantly improve nasal airflow ⁸², we regard the effects of Bernoulli forces and the stresses and strains we believe they cause to be primary in the development of the nasal cavity.

The functional matrix of the nasal cavity is air

CONCLUSION

The title of this communication extends the series of four papers published by Moss in 1997 ⁸³⁻⁸⁶. In these four papers, Moss reached out to new and exciting avenues of research that dovetailed with and supported the FMH. The merits of this forward thinking gained strength by the *American Journal of Orthodontics and Dentofacial Orthopedics* having asked Enlow to write an introduction for the first of the four papers. At that time all four papers had been written, and Enlow concludes with an expression of interest in Moss's final words on complexity in the fourth paper to be published months later.

In fact, complexity science was only just coming into mainstream thinking in the late 1990's, and it was prescient of Moss to include some remarks. There is not yet a formal definition of complexity, and the nature of such systems may even preclude one, but in general terms complex systems share the following features: They are composed of numerous parts (potentially at hierarchies of scale obeying a power law distribution), these parts are diverse, they are connected, and they are interdependent ⁸⁷. Insight is also gained by recognizing that all complex systems have a function, or purpose ⁸⁸.

Anyone who accepts this characterization will agree that the craniofacial complex is, indeed, a complex system. What is also common to complex systems is their robusticity to failure, which, in the case of the facial skeleton, is exhibited by the whole system remaining in satisfactory function even though some of the parts are perturbed, as described throughout this paper.

Perturbations exist because the *purpose* of the craniofacial complex has changed. Its purpose was to engage in chewing hard and tough food, and to breathe primarily and intensely through the nose. Changing the purpose among people of the industrialized world to chew a soft diet and, for many, to breathe through the mouth, has led to the current suboptimal health of the human population.

If you ask anyone involved in dental curricula development about the deficiencies of knowledge taught, they will lament the number of hours in a day they have to schedule student learning, but they will also ensure that course contents reflect the Boards examinations. In our view, the orthodontic community has failed to address the public health advantages of treating to the purpose of the orofacial capsules of the craniofacial complex. It is wonderful that orthodontists themselves acknowledge the risks of treatment¹¹, but it is not healthy that such risks endure by treating symptoms in deference to acknowledging causes and doing something about it. Sir Arthur Keith wrote: “Civilization... is anti-evolutionary in its effects; it works against the laws and conditions which regulated the earlier stages of man’s ascent”⁸⁹ (p. 76). If dentistry were to permit evolutionary medicine into its curriculum, then a variety of Board examination questions required for licensure can be replaced with valid ones, signifying an improvement in the health of the human population.

REFERENCES

1. Carlson DS. Craniofacial biology as “normal science”. In: Johnston LE, editor. *New Vistas in Orthodontics*. Philadelphia: Lea & Febiger; 1985. p. 12-37.
2. Moss ML. The functional matrix. In: Kraus BS, Riedel R, editors. *Vistas in Orthodontics*. Philadelphia: Lea & Febiger; 1962. p. 85-98.
3. Moss ML. Twenty years of functional cranial analysis. *American Journal of Orthodontics* 1972;61:479-485.
4. Moss-Salentijn L. Melvin L. Moss and the functional matrix. *Journal of Dental Research* 1997;76:1814-1817.
5. Moss ML, Greenberg SN. Functional cranial analysis of the human maxillary bone: I, basal bone. *Angle Orthodontist* 1967;37:151-164.
6. Moss ML, Rankow RM. The role of the functional matrix in mandibular growth. *Angle Orthodontist* 1968;38:95-103.
7. Enlow DH. A morphogenetic analysis of facial growth. *American Journal of Orthodontics* 1966;52:283-299.
8. Moss ML, Salentijn L. The primary role of functional matrices in facial growth. *American Journal of Orthodontics* 1969;55:566-577.
9. Moss ML, Salentijn L. The capsular matrix. *American Journal of Orthodontics* 1969;56:474-490.
10. Moss ML. Experimental alteration of basi-synchondrosal cartilage growth in rat and mouse. In: Bosma JF, editor. *Development of the Basicranium*. Bethesda, MD: U.S. Department of Health, Education, and Welfare; 1976. p. 541-575.
11. Perry J, Popat H, Johnson I, Farnell D, Morgan MZ. Professional consensus on orthodontic risks: What orthodontists should tell their patients. *American Journal of Orthodontics and Dentofacial Orthopedics* 2021;159:41-52.

12. Benazzi S, Kullmer O, Grosse IR, Weber GW. Using occlusal wear information and finite element analysis to investigate stress distributions in human molars. *Journal of Anatomy* 2011;219:259–272.
13. Kono RT, G.Suwa, T.Tanijiri. A three-dimensional analysis of enamel distribution patterns in human permanent first molars. *Archives of Oral Biology* 2002 47:867-875.
14. Vogel ER, Woerden JTv, Lucas PW, Atmoko SSU, Schaik CPv, Dominy NJ. Functional ecology and evolution of hominoid molar enamel thickness- Pan troglodytes schweinfurthii and Pongo pygmaeus wurmbii. *Journal of Human Evolution* 2008;55:60-74.
15. Hanaizumi Y, Maeda T, Takano T. Three-dimensional arrangement of enamel prisms and their relationship to the formation of Hunter-Schreger bands in dog tooth. *Cell and Tissue Research* 1996;286:103-114.
16. Lynch CD, O’Sullivan VR, Dockery P, McGillicuddy CT, Sloan AJ. Hunter-Schreger Band patterns in human tooth enamel. *Journal of Anatomy* 2010;217:106-115.
17. Bajaj D, Arola D. Role of Prism Decussation on Fatigue Crack Growth and Fracture of Human Enamel. *Acta Biomaterialia* 2009;5:3045–3056.
18. Chai H, Lee JJ-W, Constantino PJ, Lucas PW, Lawn BR. Remarkable resilience of teeth. *Proceedings of the National Academy of Sciences* 2009;106:7289–7293.
19. Lucas P, Constantino P, Wood B, Lawn B. Dental enamel as a dietary indicator in mammals. *BioEssays* 2008;30:374-385.
20. Boyde A. Dependence of rate of physical erosion on orientation and density in mineralized tissues. *Anatomy and embryology.* 1984;170:57-62.
21. Boyde A. Microstructure of enamel. In: Chadwick DJ, Cardew G, editors. *Dental Enamel*. West Sussex: John Wiley & Sons Ltd.; 1997. p. 18-31.
22. Shimizu D, Macho GA. Effect of Enamel Prism Decussation and Chemical Composition on the Biomechanical Behavior of Dental Tissue: A Theoretical Approach to Determine the Loading Conditions to Which Modern Human Teeth Are Adapted. *The Anatomical Record* 2008;291:175-182.
23. Stanford JW, Weigel KV, Paffenbarger GC, Sweeney WT. Compressive properties of hard tooth tissues and some restorative materials. *Journal of the American Dental Association* 1960;60:746-756.
24. Macho GA, Shimizu D. Kinematic parameters inferred from enamel microstructure: new insights into the diet of Australopithecus anamensis. *Journal of Human Evolution* 2010;58:23-32.
25. Cuy JL, Mann AB, Livi KJ, Teaford MF, Weihs TP. Nanoindentation mapping of the mechanical properties of human molar tooth enamel. *Archives of Oral Biology* 2002;47:281-291.
26. Marshall GWJ, Balooch M, Gallagher RR, Gansky SA, Marshall SJ. Mechanical properties of the dentoenamel junction: AFM studies of nanohardness, elastic modulus, and fracture. *Journal of Biomedical Materials Research* 2001;54:87-95.
27. Imbeni V, Kruzic JJ, Marshall GW, Marshall SJ, Ritchie RO. The dentin-enamel junction and the fracture of human teeth. *Nature Materials* 2005;4:229-232.
28. Zaslansky P, Friesem AA, Weiner S. Structure and mechanical properties of the soft zone separating bulk dentin and enamel in crowns of human teeth: Insight into tooth function. *Journal of Structural Biology* 2006;153 188-199.
29. Boyde A. Enamel. In: Oksche A, Vollrath L, editors. *Handbook of Microscopic Anatomy*. Berlin: Springer Verlag; 1989 p. 309-473.
30. Lacruz RS, Hacia JG, Bromage TG, Boyde A, Lei Y, Xu Y et al. The Circadian Clock Modulates Enamel Development. *Journal of Biological Rhythms* 2012;27:237-245.

31. Moreno EC, Zahradnik RT. The pore structure of human dential enamel. *Archives of Oral Biology* 1973;18:1063-1068.
32. Boyde A. Enamel structure and cavity margins. *Operative Dentistry* 1976;1:13-28.
33. Wolff J. *The Law of Bone Remodeling* (translation of the German 1892 edition). Berlin: Springer; 1986
34. Frost HM. Wolff's Law and bone's structural adaptations to mechanical usage: an overview for clinicians. *Angle Orthodontist* 1994;64:175-188.
35. Bailey CA, Kukuljan S, Daly RM. Effects of lifetime loading history on cortical bone density and its distribution in middle-aged and older men. *Bone* 2010;47:673-680.
36. Lieberman DE, Crompton AW. Responses of bone to stress. In: Weibel E, Taylor CR, Bolis L, editors. *Principles of Biological Design: The Optimization and Symmorphosis Debate*. Cambridge: Cambridge University Press; 1998. p. 78-86.
37. Wilks DC, Winwood K, Gilliver SF, Kwiet A, Chatfield M, Michaelis I et al. Bone mass and geometry of the tibia and the radius of master sprinters, middle and long distance runners, race-walkers and sedentary control participants: A pQCT study. *Bone* 2009;45:91–97.
38. Lanyon LE. Functional strain in bone tissue as an objective, and controlling stimulus for adaptive bone remodelling. *Journal of Biomechanics* 1987;20:1083-1093.
39. Dominy NJ, Vogel ER, Yeakel JD, Constantino P, Lucas PW. Mechanical Properties of Plant Underground Storage Organs and Implications for Dietary Models of Early Hominins. *Evolutionary Biology* 2008;35:159–175.
40. Agrawal KR, Lucas PW, Prinz JF, Bruce IC. Mechanical properties of foods responsible for resisting food breakdown in the human mouth. *Archives of Oral Biology* 1997;42:1-9.
41. Pereira LJ, Gaviao MBD, Bilt AVD. Influence of oral characteristics and food products on masticatory function. *Acta Odontologica Scandinavica* 2006;64:193-201.
42. Sui Z, Lucas PW, Corke H. Optimal cooking time of noodles related to their notch sensitivity. *Journal of Texture Studies* 2006;37:428–441.
43. Wikipedia. *Food Processing*. San Francisco, CA: Wikimedia Foundation, Inc.; 2020.
44. Enlow DH. *Handbook of Facial Growth*. Philadelphia: WB Saunders; 1975.
45. Brüning J, T.Hildebrandt, Heppt W, Schmidt N, Lamecker H, Szengel A et al. Characterization of the Airflow within an Average Geometry of the Healthy Human Nasal Cavity *Scientific Reports: Nature*; 2020.
46. Dallam GM, McClaran SR, Cox DG, Foust CP. Effect of Nasal Versus Oral Breathing on Vo2max and Physiological Economy in Recreational Runners Following an Extended Period Spent Using Nasally Restricted Breathing. *International Journal of Kinesiology & Sports Science* 2018;6:22-29.
47. Doorly DJ, Taylor DJ, Schroter RC. Mechanics of airflow in the human nasal airways. *Respiratory Physiology & Neurobiology* 2008;163:100–110.
48. Richerson HB, Seebohm PM. nasal airway response to exercise. *Journal of Allergy* 1968;41:269-284.
49. Zhao K, Scherer PW, Hajiloo SA, Dalton P. Effect of Anatomy on Human Nasal Air Flow and Odorant Transport Patterns: Implications for Olfaction. *Chemical Senses* 2004;29:365–379.
50. Niinimaa V, Cole P, Mintz S, Shephard RJ. The switching point from nasal to oronasal breathing. *Respiration Physiology* 1980;42:61-71.
51. Bramble DM, Lieberman DE. Endurance running and the evolution of Homo. *Nature* 2004;18:345-352.

52. Kerr WJ, McWilliam JS, Linder-Aronson S. Mandibular form and position related to changed mode of breathing--a five-year longitudinal study. *Angle Orthodontist* 1989;59:91-96.
53. Price WA. Nutrition and physical degeneration. La Mesa, CA: Price-Pottenger Nutrition Foundation; 2003.
54. Trotman CA, Jr JAM, Dibbets JM, Weele LTvd. Association of lip posture and the dimensions of the tonsils and sagittal airway with facial morphology. *Angle Orthodontist* 1997;67:425-432.
55. Jefferson Y. Mouth breathing: adverse effects on facial growth, health, academics, and behavior. *General Dentistry* 2010;58:18-25.
56. Lopatiene K, Babarskas A. [Malocclusion and upper airway obstruction] (in Lithuanian). *Medicina (Kaunas)* 2002;38:277-283.
57. Weider DJ, Baker GL, Salvatoriello FW. Dental malocclusion and upper airway obstruction, an otolaryngologist's perspective. *International Journal of Pediatric Otorhinolaryngology* 2003;67:323-331.
58. Mattar SEM, Anselmo-Lima WT, Valera FCP, Matsumoto MAN. Skeletal and occlusal characteristics in mouth-breathing pre-school children. *Journal of Clinical Pediatric Dentistry* 2004;28:315-318.
59. D'Ascanio L, Lancione C, Pompa G, El.Rebuffini, Mansi N, Manzini M. Craniofacial growth in children with nasal septum deviation: a cephalometric comparative study. *International Journal of Pediatric Otorhinolaryngology* 2010;74:1180-1183.
60. Baumann I, Plinkert PK. [Effect of breathing mode and nose ventilation on growth of the facial bones] (in German). *HNO* 1996;44:229-234.
61. Tourne LP. The long face syndrome and impairment of the nasopharyngeal airway. *Angle Orthodontist* 1990;60:167-176.
62. Deb U, Bandyopadhyay SN. Care of nasal airway to prevent orthodontic problems in children. *Journal of the Indian Medical Association* 2007;105:640, 642.
63. Harari D, Redlich M, Miri S, Hamud T, Gross M. The effect of mouth breathing versus nasal breathing on dentofacial and craniofacial development in orthodontic patients *Laryngoscope*; 2010
64. Tomer BS, Harvold EP. Primate experiments on mandibular growth direction. *American Journal of Orthodontics* 1982;82:114-119.
65. Harvold EP, Tomer BS, Vargervik K, Chierici G. Primate experiments on oral respiration. *American Journal of Orthodontics* 1981 79:359-372.
66. Elad D, Liebenthal R, Wenig BL, Einav S. Analysis of air flow patterns in the human nose. *Medical & Biological Engineering & Computing* 1993;31:585-592.
67. Eccles R. Nasal Airflow in Health and Disease. *Acta Oto-Laryngologica* 2009;120:580-595.
68. Olson LG, Strohl KP. The response of the nasal airway to exercise. *American Review of Respiratory Disease* 1987;135:356-359.
69. Maslin MA, Brierley CM, Milner AM, Shultz S, Trauth MH, Wilson KE. East African climate pulses and early human evolution. *Quaternary Science Reviews* 2014;101:1-17.
70. Svensson S, Olin AC, Hellgren J. Increased net water loss by oral compared to nasal expiration in healthy subjects. *Rhinology* 2006;44:74-77.
71. Kumar H, Jain R, Douglas RG, Tawhai MH. Airflow in the Human Nasal Passage and Sinuses of Chronic Rhinosinusitis Subjects *PLoS ONE: PLOS*; 2016.
72. Zhao K, Jiang J. What is normal nasal airflow? A computational study of 22 healthy adults. *International Forum of Allergy & Rhinology* 2014;4:435-446.
73. Lin SJ. Nasal Aerodynamics. In: Meyers AD, editor. *Medscape*; 2019.

74. Aoun L, Larnier S, Weiss P, Cazales M, Herbulot A, Ducommun B et al. Measure and characterization of the forces exerted by growing multicellular spheroids using microdevice arrays PLoS one: PLOS; 2019.
75. Asano S, Ito S, Morosawa M, Furuya K, Naruse K, Sokabe M et al. Cyclic stretch enhances reorientation and differentiation of 3-D culture model of human airway smooth muscle. *Biochemistry and Biophysics Reports* 2018;16:32-38.
76. Codelia VA, Sun G, Irvine KD. Regulation of YAP by Mechanical Strain through Jnk and Hippo Signaling. *Current Biology* 2012;24:2012-2017.
77. Wang JG, Miyazu M, Xiang P, Li SN, Sokabe M, Naruse K. Stretch-induced cell proliferation is mediated by FAK-MAPK pathway. *Life Sciences* 2005;76:2817–2825.
78. Jaslow CR. Mechanical properties of cranial sutures. *Journal of Biomechanics* 1990;23:313-321.
79. Endo B. Distribution of stress and strain produced in the human facial skeleton by the masticatory force. *Zinrugaku Zassi* 1965;73:9-21.
80. Hsu H-Y, Yamaguchi K. Decreased chewing activity during mouth breathing *Journal of Oral Rehabilitation: Blackwell Publishing Ltd*; 2012.
81. Glanville EV. Nasal shape, prognathism and adaptation in man. *American Journal of Physical Anthropology* 1969;30:20-38.
82. Wertz RA. Changes in nasal airflow incident to rapid maxillary expansion. *Angle Orthodontist* 1968;38:1-11.
83. Moss ML. The functional matrix hypothesis revisited. 1. The role of mechanotransduction. *American Journal of Orthodontics and Dentofacial Orthopedics* 1997;112:8-11.
84. Moss ML. The functional matrix hypothesis revisited. 2. The role of an osseous connected cellular network. *American Journal of Orthodontics and Dentofacial Orthopedics* 1997;112:221-225.
85. Moss ML. The functional matrix hypothesis revisited. 3. The genomic thesis. *American Journal of Orthodontics and Dentofacial Orthopedics* 1997;112:338-342.
86. Moss ML. The functional matrix hypothesis revisited. 4. The epigenetic antithesis and the resolving synthesis. *American Journal of Orthodontics and Dentofacial Orthopedics* 1997;112:410-417.
87. Page SE. *Diversity and Complexity*. Princeton, NJ: Princeton University Press; 2011.
88. Meadows DH. *Thinking in Systems: a primer*. White River Junction, VT: Chelsea Green Publishing Company; 2008.
89. Keith A. *Evolution and Ethics*. New York: G.P. Putnam's Sons; 1047.